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# Polycrystalline silicon ion sensitive field effect transistors

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We report the operation of polycrystalline silicon ion sensitive field effect transistors. These devices can be fabricated on inexpensive disposable substrates such as glass or plastics and are, therefore, promising candidates for low cost single-use intelligent multisensors. In this work we have developed an extended gate structure with a  $\text{Si}_3\text{N}_4$  sensing layer. Nearly ideal  $\text{pH}$  sensitivity ( $54 \text{ mV/pH}$ ) and stable operation have been achieved. Temperature effects have been characterized. A penicillin sensor has been fabricated by functionalizing the sensing area with penicillinase. The sensitivity to penicillin G is about  $10 \text{ mV/mM}$ , in solutions with concentration lower than the saturation value, which is about  $7 \text{ mM}$ . © 2005 American Institute of Physics.

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The use of ion-sensitive field effect transistors (ISFETs) to measure  $\text{pH}$  and to sense a variety of ions is well known.<sup>1</sup> In these devices the gate insulator is in direct contact with the electrolyte solution. The high surface buffer capacity of the insulator<sup>1</sup> leads to an almost constant proton density at the surface, independently of the electrolyte's  $\text{pH}$ . Hence a  $\text{pH}$ -dependent potential drop across the double layer arises, in order to equalize the free energy difference for protons at the interface and in the bulk of the solution, resulting in modulation of the channel conductance.

By coating the gate insulator with enzymes as the selecting agent, highly selective sensors have been developed.<sup>2</sup> Such enzyme-modified ISFETs (EnFETs) can in principle be constructed with any enzyme that upon reaction with the analyte induces a local change of  $\text{pH}$ . ISFET biosensors are used in medical diagnostics, environmental monitoring, and food quality control. One distinctive advantage of ISFETs is their suitability for miniaturization, since the signal to noise ratio is independent of the ISFET area. Therefore large multisensor arrays capable of detecting different species and simultaneously measuring relevant parameters (temperature,  $\text{pH}$ , etc.) are possible. In all these applications cost and single-use, that is disposability, are paramount considerations.

We report here the use of extended gate polycrystalline silicon thin film transistors (poly-Si TFTs) as ISFETs and penicillin sensitive EnFETs. The poly-Si TFT technology is well established in the area of flat panel displays. In addition to the pixel switching array, where typically some  $10^6$  poly-Si TFTs are employed, complex integrated circuits, such as logic drivers and SRAMs can be fabricated with these devices. Furthermore, these circuits can be made on inexpensive disposable substrates such as glass or plastic.<sup>3</sup> Poly-Si TFTs are, therefore, promising candidates for low cost single-use intelligent multisensors. In view of the fact that the device is used in an aqueous environment, an added advantage of this technology over conventional bulk CMOS

is the electrical isolation between the individual transistors.

The inset in Fig. 1 shows the schematic structure of the extended gate ISFET. The devices were fabricated on glass substrates by laser recrystallization.<sup>3</sup>  $\text{Si}_3\text{N}_4$  was deposited by plasma enhanced chemical vapor deposition (PECVD) on top of the tantalum extended gate, to serve as the  $\text{pH}$  sensitive layer. To provide electrical and chemical isolation, the entire device area, except the sensitive  $\text{Si}_3\text{N}_4$  pad, was passivated with a  $\text{Si}_3\text{N}_4$ (100 nm)/ $\text{SiO}_2$ (500 nm) layer.  $\text{p}$ -channel TFTs with different gate sizes have been fabricated and tested. The channel length of the TFTs is  $6 \mu\text{m}$ , while the channel widths range between 10 and  $100 \mu\text{m}$ . The sensing pad area is  $1 \text{ mm} \times 1 \text{ mm}$ .

For the penicillin EnFET, the enzyme penicillinase was adsorptively immobilized on the surface of the  $\text{Si}_3\text{N}_4$  pad. For the immobilization, the enzyme solution was prepared by dissolving 2000 units of enzyme penicillinase in 1 ml of 50 mM phosphate buffer with  $\text{pH}$  7.5.  $10 \mu\text{l}$  of enzyme solution was pipetted onto the chip, covering one  $\text{Si}_3\text{N}_4$  pad, and incubated for 1 h at room temperature. The sample was then rinsed and dried at room temperature. The penicillin G solu-

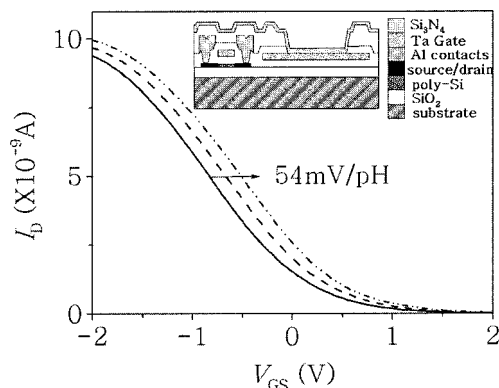


FIG. 1.  $I_D$ - $V_{GS}$  curve for a  $\text{p}$ -type ISFET with transistor size  $W/L = 20 \mu\text{m}/6 \mu\text{m}$  measured with  $V_{DS} = 0.1 \text{ V}$  in phosphate buffer with different  $\text{pH}$  values (from left to right:  $\text{pH} = 4.0, 7.0$  and  $10.0$ ). Inset: Schematic structure of the extended gate ISFET.

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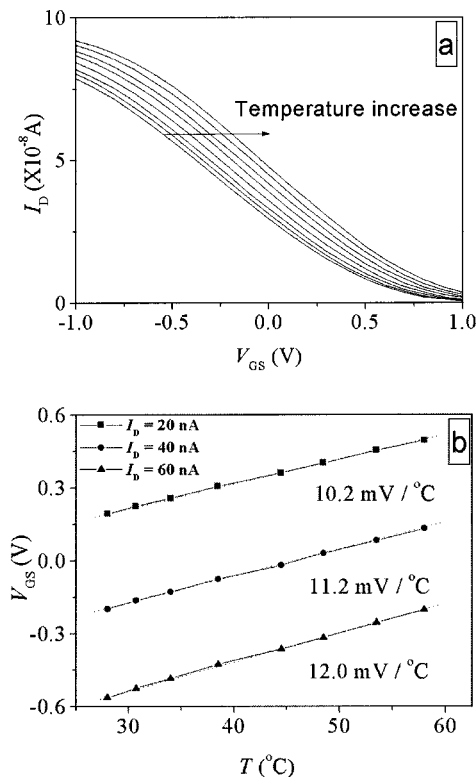


FIG. 2. (a)  $I_D$ - $V_{GS}$  curve of a  $p$ -type ISFET with transistor size  $W/L = 100 \mu\text{m}/6 \mu\text{m}$ , measured with  $V_{DS} = 0.1 \text{ V}$  in a 5 mM phosphate buffer  $p\text{H} 7.6$  at different temperatures. The temperatures corresponding to the curves from left to right are 28.0, 30.7, 34.0, 38.5, 44.5, 48.5, 53.5, and 58.0 °C, respectively; (b) temperature dependence of the gate voltage corresponding to the different values of  $I_D$ .

tions were prepared in different concentrations, using a 5 mM phosphate buffer with  $p\text{H} 7.0$ . After each concentration step, the sensor was rinsed with the working buffer. Phosphate buffer, penicillinase, penicillin G were purchased from Sigma-Aldich.

The  $I_D$ - $V_{GS}$  characteristics of the ISFETs and penicillin EnFET were measured using a HP4378 parameter analyzer. An Ag/AgCl reference electrode was used. During the measurements,  $V_{DS}$  was kept constant at 0.1 V and  $V_{GS}$  was swept from negative voltage to positive voltage and back. It was found that in order to avoid transient effects due to the sensor response, the sweeping speed had to be lower than 0.1 V/s. So the sensor response time to  $V_{GS}$  change is of the order of 1 s, which can be attributed to the mechanism at the  $\text{Si}_3\text{N}_4$ /electrolyte interface, since the TFT response is much faster.

The  $I$ - $V$  curves are very stable and repeatable and show a rigid shift with the change of  $p\text{H}$  value. The voltage shift is proportional to the change in  $p\text{H}$ . Typical characteristics are shown in Fig. 1 for a TFT with  $W/L = 20 \mu\text{m}/6 \mu\text{m}$ . The  $p\text{H}$  sensitivity is 54 mV/ $p\text{H}$  at 300 K, close to the ideal value of 59 mV/ $p\text{H}$ .<sup>4</sup> In some cases a lower  $p\text{H}$  sensitivity, between 47 and 54 mV/ $p\text{H}$  was observed. It is expected from the site-binding theory<sup>5</sup> that the state of the surface of the  $\text{Si}_3\text{N}_4$  is critical for the  $p\text{H}$  sensing properties. Impurities, such as oxygen or other ions, which might exist at the  $\text{Si}_3\text{N}_4$  surface<sup>6</sup> can result in a nonideal sensitivity. Further investigation of these aspects is needed.

The temperature dependence of the ISFET characteristics has been measured using a 5 mM phosphate buffer with  $p\text{H} 7.6$  and is shown in Fig. 2(a) for a TFT with  $W/L$

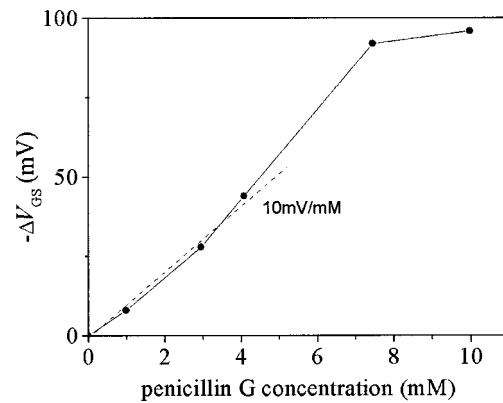


FIG. 3. Gate voltage shift  $\Delta V_{GS}$  taken from the  $I_D$ - $V_{GS}$  curves of a  $p$ -type EnFET with transistor size  $W/L = 100 \mu\text{m}/6 \mu\text{m}$  measured in a 5 mM phosphate buffer  $p\text{H} 7.0$  vs penicillin G concentration.

$= 100 \mu\text{m}/6 \mu\text{m}$ . Both threshold voltage and shape of the  $I$ - $V$  curves change with temperature. Figure 3 shows the voltage shift versus temperature for three values of  $I_D$ . The behavior is linear and the temperature coefficients for the three curves are slightly different. The temperature coefficient is higher than the one observed for single crystal ISFETs.<sup>7</sup> There are three main possible contributions to the observed temperature effect: (1) temperature-dependent potential change at the Ag/AgCl reference electrode; (2) temperature-dependent potential drop at the  $\text{Si}_3\text{N}_4$ /electrolyte interface; (3) temperature-dependent poly-Si TFT characteristics. The first two contributions can only induce a parallel shift of the  $I$ - $V$  curves, while the third one can also change the shape of the  $I$ - $V$  curve itself.

The temperature dependence of the potential at Ag/AgCl reference electrodes has been reported to be on the order of 0.14 mV/K.<sup>7</sup> On the other hand, the potential drop  $\varphi_0$  at the interface between  $\text{Si}_3\text{N}_4$  and the electrolyte is, according to site-binding theory,<sup>1,4,5</sup>

$$\varphi_0 = 2.3 \frac{kT}{q} \frac{\beta}{\beta + 1} (p\text{H}_{pzc} - p\text{H}),$$

where  $p\text{H}_{pzc}$  is the  $p\text{H}$  value at the point of zero charge in the interface,  $k$  is the Boltzmann constant,  $q$  is the electronic charge,  $T$  is the temperature of the system, and  $\beta$  is a parameter, which can be expressed in terms of the acidic and basic equilibrium constants of the related surface reactions. Using the value of  $p\text{H}_{pzc} = 5.2$  for  $\text{Si}_3\text{N}_4$ ,<sup>5</sup> the temperature coefficient becomes 0.48 mV/K at  $p\text{H} 7.6$ . The values for the temperature coefficients for the first two possible contributions described above are much smaller than the experimentally observed one. This value is consistent with the temperature dependence of poly-Si TFT  $I$ - $V$  characteristics. This dependence is controlled by the gap density of states, which is fairly reproducible in a stable process. Therefore a reference TFT can be used as a temperature sensor and to provide the input for temperature compensation.

For the penicillin EnFET, penicillinase was immobilized on the  $\text{Si}_3\text{N}_4$  gate dielectric. The functionalized ISFET detects the variation in  $\text{H}^+$  concentration, resulting from the catalyzed hydrolysis of penicillin by penicillinase, which is dependent on the penicillin concentration in the solution.<sup>2,8</sup> Figure 3 shows the voltage shift, measured in 5 mM  $p\text{H} 7.0$  phosphate buffer versus penicillin G concentrations. The  $I$ - $V$  curves shift to negative voltages for increasing penicillin

concentration. The shift is linear with concentration until saturation is reached at about 7 mM. The sensitivity is 10 mV/mM.

In conclusion, we have fabricated ISFETs on glass substrates, by using low-temperature Poly-Si TFT technology. An extended gate structure has been developed, using PECVD  $\text{Si}_3\text{N}_4$  as the pH sensitive area. Stable operation and nearly ideal pH characteristics have been obtained. A penicillin G sensor has been fabricated by functionalizing the  $\text{Si}_3\text{N}_4$  with penicillinase. The extended gate structure facilitates the electrical and chemical isolation of the sensor, hence increasing its stability and durability. This technology, in view of the advanced level of development for mass production of polysilicon TFTs and the use of cheap substrates such as glass or plastics, shows great promise for application in single-use multi-analyte biosensors.

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